

Exploiting disorder for perfect focusing

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We demonstrate experimentally that disordered scattering can be used to improve, rather than deteriorate, the focusing resolution of a lens. By using wavefront shaping to compensate for scattering, light was focused to a spot as small as one tenth of the diffraction limit of the lens. We show both experimentally and theoretically that it is the scattering medium, rather than the lens, that determines the width of the focus. Despite the disordered propagation of the light, the profile of the focus was always exactly equal to the theoretical best focus that we derived.

Optical microscopy and manipulation methods rely on the ability to focus light to a small volume. However, in inhomogeneous media, such as biological tissue, light is scattered out of the focusing beam. Disordered scattering is thought to fundamentally limit the resolution and penetration depth of optical methods [1, 2, 3]. Here we demonstrate in an optical experiment that this very scattering can be exploited to improve, rather than deteriorate, the sharpness of the focus. Surprisingly, the resulting focus is even sharper than in a transparent medium. By using scattering in the medium behind a lens, light was focused to a spot as small as one tenth of the diffraction limit of that lens. Our results, obtained using spatial wavefront shaping, are valid for all methods for focusing coherent light through scattering matter, including phase conjugation[4] and time-reversal[5]. We anticipate that disorder-assisted focusing will improve the imaging resolution of microscopy in inhomogeneous media.

The starting situation of the experiment is shown in Fig. 1a: a lens focuses a beam of light onto a CCD camera. In this ‘clean’ system without disorder, the sharpness of the focus is limited by the numerical aperture and the quality of the lens. We now disturb the light propagation by placing a non-transparent scattering object in the beam path. Although initially the focus disappears, the focus can be restored by shaping the wavefront of the incident light using a spatial light modulator[6] (see Fig. 1b). Here we report and analyze a surprising property of the restored focus: the experimentally obtained focal spot is smaller than the diffraction limit of the clean system. We show both experimentally and theoretically that it is the scattering medium, rather than the lens or the quality of the reconstruction process, that determines the width of the focus.

In Fig. 2a we show the measured intensity distribution in the focal plane of the clean system. Ideally, the lens would focus light to an Airy disk with a full width at half maximum (FWHM) of $w = 1.03\lambda f_1/D_1$. In our experiment, $\lambda = 632.8$ nm, $f_1 = 200$ mm, and $D_1 = 2.1$ mm,

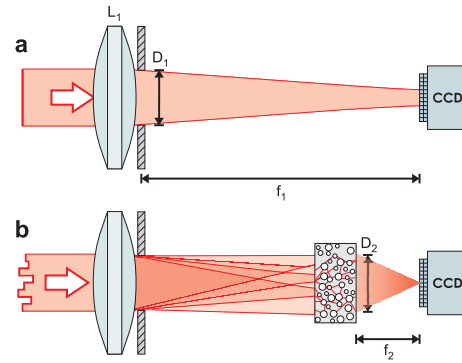


FIG. 1: Schematic of the experiment. Light coming from a phase modulator is imaged on the centre plane of a lens, L_1 (modulator and imaging telescope not shown). The numerical aperture of the lens is controlled by a pinhole. A CCD camera is positioned in the focal plane of the lens. (a), ‘Clean’ system without disorder. Light is focused to a spot that is, at best, equal to the diffraction limit of the lens. (b), System with disorder. A disordered sample randomly changes the direction of the incident light. The scattering object can be moved to change the distance to the camera. When the incident wavefront is shaped to create a focus through the sample, the resulting focus is sharper the best focus the lens can create without disorder.

which gives a diffraction limited spot size of $62\ \mu\text{m}$. In reality [7], the focus has a slightly larger width of $76 \pm 3\ \mu\text{m}$. When the beam path is blocked by a disordered medium (a $6\ \mu\text{m}$ layer of opaque white airbrush paint), the image on the camera changes dramatically. Instead of a focus, we now record a disordered speckle pattern (see Fig. 2b). Typically, the light is scattered and diffracted about a hundred times before reaching the other side of the sample. Therefore, the transmitted wave has lost all correlation with the incident wavefront[8], and the efficient wavefront correction systems that have been developed

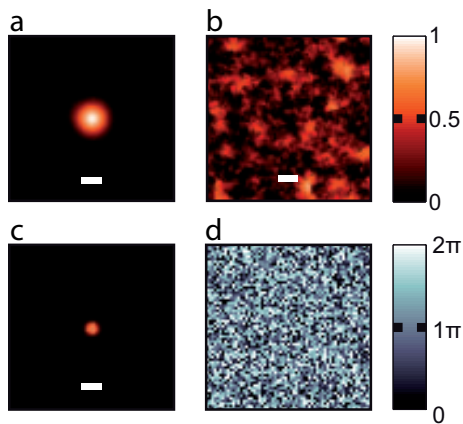


FIG. 2: Measured intensity distribution in the focal plane at 200 ± 3 mm from the glass lens. (a), Clean system with an unmodified incident wavefront. The focal width is of the order of the diffraction limit ($62 \mu\text{m}$, white bar). (b), System with the $6 \mu\text{m}$ layer of airbrush paint present, unmodified incident wavefront. No focus is discernible. (c), System with the sample present, wave was shaped to achieve constructive interference in the target. A high-contrast, extremely sharp focus is visible. (d), Pattern on the spatial phase modulator for the situation in Fig. c. The intensity plots are normalized to the brightest point in the image.

in adaptive optics cannot be used[9].

We recover the focus using an approach that was designed specifically for strongly scattering environments. A spatial light modulator shapes the wavefront of the light that impinges on the lens. The surface area of the light modulator was subdivided into 64×64 square segments, which are phase-modulated[10] and controlled by a learning feedback algorithm[7]. The algorithm adjusts the relative phases of the segments so that the transmitted light interferes constructively in a chosen target, thereby creating a focus at that point. In this case, the target was formed by a single $6.45 \mu\text{m} \times 6.45 \mu\text{m}$ CCD pixel in the centre of the desired focus. The algorithm finds the optimal wavefront for focusing on this target (see Fig. 2d). The optimal wavefront is completely disordered, which confirms that the sample is strongly scattering.

In Fig. 2c we show the intensity distribution after running the algorithm. The scattered light now focuses to a tight spot, even though the algorithm did not optimize the shape of the focus explicitly. What is more, the width of this spot is approximately one tenth of the diffraction limit of the lens: scattering has greatly improved the focusing resolution.

To analyze this striking effect, we placed the sample at different distances f_2 from the camera. In Fig. 3 we show the width of the focus in these experiments. The widths decrease as the sample is moved closer to the camera,

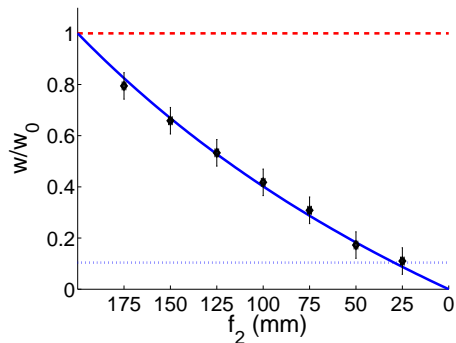


FIG. 3: Focal width w , relative to the diffraction limit of the glass lens ($w_0 = 62 \mu\text{m}$, dashed line), as a function of the distance f_2 between the scattering sample and the focal plane. Diamonds, measured values with a sample present; solid curve, theoretical effective diffraction limit (no free parameters); dotted line, size of a single pixel of the camera.

and are always smaller than the width of the diffraction limited spot of the clean system. At distances of 25 mm or smaller, the width of the focus is smaller than a single camera pixel, almost a factor ten below the diffraction limit of the lens.

We proceed to quantitatively define an effective diffraction limit for a scattering system. We will show below that the width of the smallest achievable focus is given by the FWHM of an Airy disc

$$w = 1.03\lambda f_2 / D_2, \quad (1)$$

with f_2 the distance between the scattering layer and the focal plane and D_2 the diameter of the illuminated area on the scattering layer[7].

In Fig. 3 we plot our theoretical effective diffraction limit as a function of the distance between the scattering layer and the focal plane. The theoretical limit decreases almost linearly as the sample is moved closer to the chosen focus. With no adjustable parameters, the experimentally observed focal widths equal the theoretical lower limit that our model predicts.

To understand why the scattered light focuses to exactly the theoretically smallest possible focus - even though no effort is made to explicitly minimize the width of the focus - we now calculate how a shaped wavefront propagates through a scattering sample. The propagation of light from a source at \mathbf{r}_a to a target at \mathbf{r}_β through a sample is described by the stochastic Green function $G(\mathbf{r}_\beta, \mathbf{r}_a)$. Theoretically[11, 12], the maximum intensity transmission is achieved when the incident field $E(\mathbf{r}_a)$ is modulated spatially so that $E(\mathbf{r}_a) \propto G^*(\mathbf{r}_\beta, \mathbf{r}_a)$, where $*$ denotes the complex conjugate. Our algorithm constructs this wavefront by maximising the intensity at point \mathbf{r}_β . This is the same wavefront that one would

get when one would phase conjugate the light[4] coming from a (hypothetical) source at \mathbf{r}_β .

If all channels on both sides of the sample could be controlled, the light would form a perfect spherical wave[11] that converges to point \mathbf{r}_β . In a transmission geometry, only a finite number of channels on one side of the sample are controlled. Therefore it is, even in principle, impossible to perfectly focus all incident light. However, since the sample completely scrambles the incident wavefront, any deviation from the perfect wave is randomly distributed over all outgoing angles. Therefore, the average field at the back of the sample still constitutes a converging spherical wave originating from the illuminated part of the sample[7]

$$\langle E(\mathbf{r}_k; \mathbf{r}_\beta) \rangle = g^*(\mathbf{r}_\beta - \mathbf{r}_k) C_0 I_0(\mathbf{r}_k), \quad (2)$$

where $E(\mathbf{r}_k; \mathbf{r}_\beta)$ denotes the field at point \mathbf{r}_k on the back of the sample after programming the modulator to optimize the intensity in target \mathbf{r}_β . g is the Green function for propagating through air, C_0 is a constant to normalize the total incident power, and $I_0(\mathbf{r}_k)$ is the ensemble averaged intensity distribution at the back of the sample. Equation 2 shows that experimental limitations do not change the shape of the focus, they merely cause the contrast with the speckle background to decrease.

The term $I_0(\mathbf{r}_k)$ in Eq. 2 acts as an effective aperture function for the scattering ‘lens’. In our experiments $I_0(\mathbf{r}_k)$ is approximated well by a top hat disk with a diameter of D_2 . In this case, Eq. 2 describes diffraction limited focusing at point \mathbf{r}_β by a lens with a clear aperture of D_2 . This result explains the experimental observation in Fig 3 that the focal width always equals the theoretical minimum.

The intensity distribution in the focal plane is found from Eq. 2 by paraxially propagating the field. We derived[7]

$$I(\mathbf{r}_b; \mathbf{r}_\beta) = S_I |\mathcal{F}\{I_0(\mathbf{r}_k)\}|^2, \quad (3)$$

with $\mathcal{F}\{\}$ the two-dimensional Fourier transform, and S_I a normalization constant that is fixed by the condition that $I(\mathbf{r}_\beta; \mathbf{r}_\beta) = I_0(\mathbf{r}_\beta)(\pi(N-1)/4+1)$, with N the number of independent modulator segments and I_0 the average intensity of the diffuse background before optimization[6, 12]. The intensity in the focus increases linearly with the number of segments, until N is equal to the total number of degrees of freedom of the optical field.

Equation 3 predicts the shape of the reconstructed focus. Surprisingly, this equation takes the same form as the van Cittert-Zernike theorem[13, 14, 15]. This theorem tells us that the speckle correlation function is proportional to $|\mathcal{F}\{I_0(\mathbf{r}_k)\}|^2$. Our derivations suggest an alternative interpretation of this decades-old theorem: the theorem predicts the exact shape to which a disordered sample will focus an optimized wavefront.

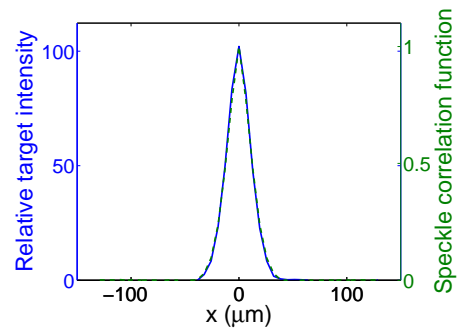


FIG. 4: Intensity profile of the focus at $y = 0$ (solid curve) and speckle correlation function (dashed curve) for an $6\mu\text{m}$ thick layer of airbrush paint creating a focus at 10.0 cm distance. The speckle correlation function was measured with a randomly generated incident wavefront.

To test this remarkable result, we compare the measured shape of the reconstructed focus to the measured auto-correlate of the background speckle. In Fig. 4 the two normalised curves can be seen to overlap perfectly. We repeated this experiment in different geometries and with different samples and found that the shape of the focus is always in agreement with the shape that the van Cittert-Zernike theorem predicts.

In conclusion, scattering in a medium behind a lens can be used to *improve* the focusing resolution to beyond the diffraction limit of that lens. We found that, surprisingly, the shape of the focus is not affected by experimental limitations of the wavefront modulator: the focus is always exactly as sharp as is theoretically possible.

Disordered scattering has been applied to improve resolution and bandwidth in imaging and communication with ultrasound, radio waves and microwaves[5, 16, 17], and significant sub-wavelength effects have been demonstrated [18]. Our results are the first demonstration that similar resolution improvements can be obtained in photonics. Calculations [19, 20] indicate that useful optical superresolution will be achieved using disordered plasmonic nanostructures.

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